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Prof. Dr Abhay Datarkar, MDS, DNB, FIBCOMS, Dr Shikha Tayal, MDS, Junior Resident, Mr Abhishek Thote, Research Scholar, Dr Manlio Galie, MD, DMD, FEBOMFS

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An in-vitro evaluation of a novel design of miniplate for fixation of fracture segments in the transition zone of parasymphysis-body region of mandible using finite element analysis

Corresponding author

Prof. Dr Abhay Datarkar

MDS, DNB, FIBCOMS

Department of Oral and Maxillofacial Surgery

Government Dental College & Hospital,

Medical campus, Medical Square,

Nagpur, Maharashtra, India

Contact no: (+91) 9822698145, 0712 2283888

E-mail: abhaydatarkar@yahoo.com

2nd author

Dr Shikha Tayal

MDS (Junior Resident)

Department of Oral and Maxillofacial Surgery,

Government Dental College, Nagpur,

Maharashtra, India – 440003

Email: daringshikha@gmail.com

3rd author

Mr Abhishek Thote

Research Scholar,

Department Of Mechanical Engineering, VNIT, Nagpur,

Maharashtra, India

Email: abhi.thote8@gmail.com

4th author

Dr Manlio Galie

MD, DMD, FEBOMFS

EACMF Education and Training Officer

Director and Chief, Unit of CranioMaxilloFacial Surgery

St Anna Hospital and University

Viale Aldo Moro, 8 44124

Ferrara – Cona, Italy

Manlio.galie@unife.it

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SUMMARY

The mandibular parasymphysis and body regions are highly dynamic areas. They are constantly subjected to both occlusal and muscular forces. Fractures at this transition zone of the parasymphysis and body region thus represent a special pattern that creates a dilemma for the surgeons — whether to use one miniplate fixation or two miniplates as per Champy's guidelines. Mental nerve paresthesia is a very common complication due to dissection and stretching of the mental nerve in this region. Hence, an in-vitro research study of a novel twin fork design of miniplate is performed, which evaluates the biomechanical behavior using computerized finite element analysis. A comparison is carried out with the conventional design. The results show that the twin fork miniplate produces the lowest stresses — 23.821 MPa — and the least total structural deformation after applying the maximum occlusal bite force. This study concludes that the newly designed miniplate is superior in terms of stability because it shows the least structural deformation, and produces the lowest equivalent stresses on application of maximal occlusal forces. An additional advantage is the preservation of the mental nerve during the plating procedure because the broad end of the Y shape allows atraumatic positioning of the miniplate and hence the fixation of fractured segments.

Keywords: finite element analysis; biomechanical evaluation; miniplate; internal fixation; mental nerve paresthesia

22

INTRODUCTION

23 Fractures through the mandible at the level of the parasymphysis, extending obliquely and
24 traversing through the transitional zone to the body region, are relatively common and account
25 for approximately 20% of mandibular fractures¹. The mandibular parasymphysis and body
26 regions are highly dynamic areas, constantly subjected to various types of occlusal and muscular
27 force. It is well known that the mandible is normally subjected to tension forces on its superior
28 border and compression forces on its inferior border²⁻⁵. Torsional forces are also created within
29 the mandibular parasymphysis, which increases in strength towards the midline. However, there
30 is disruption of the dynamics when a fracture occurs, causing the fracture segments to be
31 subjected to various types of stress.

32 Anatomically, the transition zone is characterized by the presence of deeper roots, neurovascular
33 bundle and associated mental foramen, and a change in density and orientation of the bony
34 trabeculae due to the gradual change in the arch form of the mandible. These all contribute to a
35 different clinical picture and, consequently, a different pattern of fractures in this zone,
36 necessitating a different approach to management. Fractures in the transition zone of the
37 parasymphysis and body region thus represent a special pattern that creates a dilemma for the
38 surgeons — whether to use one miniplate fixation or two miniplates as per Champy's guidelines.
39 Moreover, mental nerve paresthesia is a very common complication due to dissection and
40 stretching of the mental nerve in this region⁶. Additionally, trauma itself may compromise the
41 neurovascular function of the mental nerve.

42 Hence, a novel design of the conventional miniplate has been created with the aim of resolving
43 this dilemma and additionally minimizing damage to the neurovascular bundle due to the plating

44 technique. An in-vitro study is performed that evaluates the biomechanical behavior of the newly
45 designed titanium miniplate using finite element analysis. This design promises to follow
46 Champy's lines of osteosynthesis, as well as provide better stability and fixation properties
47 compared with the conventional design.

48 Finite element analysis (FEA) is a computed technique originally developed by engineers to
49 model the mechanical behavior of complex structures, ranging from buildings to human
50 anatomical body parts. A numerical approach simplifies a complex shape with infinite degrees of
51 freedom into a number of simpler, finite, interconnected shapes or elements. The accuracy of this
52 approach is dependent on many variables, including the accuracy of geometric replication, and
53 the number and complexity of the elements used in the model. As there are a limited (finite)
54 number of elements in a given model, the analysis is termed finite element analysis. FEA has
55 been used previously to evaluate the treatment of facial fractures^{7, 8}, and its use in evaluating
56 plating techniques has been established⁸.

57 The aim of this study is to evaluate the performance of the newly designed miniplate in terms of
58 structural deformation and production of equivalent von Mises stresses, and to compare it with
59 the conventional design using computerized FEA.

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MATERIALS AND METHODS

63 This study analyzes the biomechanical behavior of a newly designed, twin-fork-shaped miniplate
64 used for the internal fixation of fracture of the mandible at the transition zone of the
65 parasymphysis and body region, and compares it with the conventional design. For this purpose,

66 a three-dimensional finite element model of the mandible was developed. The type and
67 positioning of the miniplates were determined in accordance with the clinical application.

68

69 **1. Construction of the basic finite element model of mandible**

70 The three-dimensional finite element computer model was generated on the basis of
71 measurements from a human cadaveric model of the mandible using the software Creo version
72 2.0. The constructed model was equivalent to the real shape and size of the mandible, and an *xyz*
73 coordinate system was assigned to the model such that the *x* direction was antero-posterior, the *y*
74 direction was supero-inferior, and the *z* direction was medio-lateral.

75 The geometry data were imported into a generally accepted, and already commercially available,
76 FEM program, ANSYS WORKBENCH 16. In our FE modeling, the anatomical specifications
77 for the mandible were simplified by not considering the teeth. The properties of the bone were
78 assumed to be isotropic, homogenous, and linearly elastic. The behavior of the bone was
79 characterized by two constants (Young modulus and Poisson ratio). The average values already
80 mentioned and approved in the literature⁹ were attained. Young modulus was taken as 13 700
81 MPa, and Poisson ratio was 0.26.

82

83 **2. Construction of finite element model of titanium plates with screws**

84 The dimensions and specifications of the different designs of conventional titanium miniplate
85 were entered into the software (Creo, version 2.0), and three-dimensional models of the
86 miniplates along with the screws were created with exact geometry (Figure 1). Material
87 properties for titanium were assigned as 110 000 MPa for Young modulus and 0.34 for Poisson
88 ratio (strain limit-0.2%)¹⁰. The fracture site in the transition zone of the parasymphysis-body

89 region was determined and different assemblies of miniplate were applied as per the clinical
90 protocol defined by Champy. Perfect adaptation between miniplates/screws and the bone, with
91 no slippage at their interfaces, was considered, along with the fixed contact of the miniplate with
92 the bone, to evaluate the stresses transferred to the miniplate along the bone. The volume
93 elements of ANSYS were meshed and elements obtained. The solid element type 10-node
94 tetrahedron and 20-node hexahedron was chosen to model the bone segments, with three
95 translations in the nodal x , y , and z directions per node (Figure 2).

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3. Occlusal loading

98 A bite force of 570 N was applied over the occlusal surface of the generated model while
99 keeping the condylar and coronoid processes fixed. Though the normal functional occlusal forces
100 without any fracture of mandible, as well as in fractured mandible cases, are far less, the
101 maximum occlusal force that can be possibly loaded in a mandible was taken in order to measure
102 the biomechanical changes in the miniplates as well as the hosting bone.

103 With an adequate and simplified geometric finite element model and the appropriate material
104 properties, along with the highest occlusal loading and support conditions (Figure 3), the finite
105 element solver module of the ANSYS software carried out the mathematical procedure, and
106 displacement and stress values for each node as well as element were obtained.

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4. Finite element analysis

109 On application of the highest occlusal forces, the total structural deformation of the miniplates
110 and screws, along with the bone and von Mises (VM) stresses generated, were obtained and
111 recorded for each configuration of miniplate and screws using the computerized software. By

112 analyzing the VM stresses predicted by the model for each configuration, and the total structural
113 deformation of the miniplates in each configuration, we could analyze which configuration of
114 miniplate and screws provided the greatest stability. VM stress is a value used to determine
115 whether a given material will yield or fracture under a given load. If the VM stress is greater, the
116 material is expected to yield or fracture. Hence, configurations with the lowest relative VM stress
117 and the least structural deformation were likely to be the most stable.

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RESULTS

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1. Total structural deformation

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2. Equivalent von-Mises stresses

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The equivalent VM stresses generated for the various configurations are depicted in Figure 5. These were calculated to predict yielding in the fixation units (plates and screws). The results showed that the twin-fork miniplate produced the lowest stress — 23.821MPa — on occlusal loading, and had the least chance of yielding when compared with the other two miniplate configurations. The maximum stress was generated by the two-miniplate design (76.92 MPa). The VM stress value for the single miniplate was 76.23 MPa. This showed that our newly designed twin-fork miniplate, even on application of maximum forces, can provide the best stability.

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DISCUSSION

137 As a result of dynamic biomechanics, the behavior of various patterns of stresses, and the forces
138 generated in the transition zone of the body and parasymphysis of the mandible, there is always a
139 dilemma for the surgeons as to whether to fix the mandibular segments with one or two
140 miniplates. The presence of the mental nerve in this region makes it more challenging for the
141 surgeons to fix the fracture segments without dissecting and damaging the nerve. This new
142 miniplate is therefore designed to overcome these issues.

143 Evaluation of the biomechanical behavior of this new miniplate using finite element analysis
144 revealed that this newly designed miniplate is superior in terms of stability. The structural
145 deformation for this design of miniplate was the lowest of those studied and, further, produced
146 the lowest equivalent VM stresses on application of maximum occlusal forces. Thus, it reduces
147 the yielding of the fixation units under stresses, and restricts any micromovements in the fracture
148 segments as well as in the miniplate/screws and associated bone. This more rigid fixation should
149 lead to faster healing.

150 Additional advantages include preservation of the mental nerve during the plating procedure and,
151 as a result of the broad end of the Y-shaped miniplate, atraumatic positioning of the miniplate
152 and hence fixation of fractured segments. Although improper handling of the soft tissues may
153 cause neurosensory disturbances, only gentle reflection of the periosteum is required in order to
154 insert the twin-fork-shaped miniplate in the inframental foramen region.

155 Another mechanical advantage of this specific design is the equal distribution of the vector
156 forces and stresses along the three arms. As a result, forces along the inner zone of the broad end
157 of the Y shape are neutralized, with the neutral zone overlying the anatomical location of the

158 mental nerve. The miniplate can also be adapted according to the exact location of the fracture
159 line in order to achieve similar results (Figure 6).

160 There are two limitations of this study:

- 161 1. There are inherent limitations in the finite element model because of its geometrical
162 simplification/idealization, material characteristic properties, and boundary conditions¹¹.
- 163 2. Further anatomical variations of the mandible and fracture cannot be considered in the
164 analysis.

165 The interim results of this finite element analysis study are very encouraging, leading to the
166 conclusion that the new miniplate is better in terms of stability. Further in vivo, long-term studies
167 continue in the department, where clinical utility and outcome are being evaluated in terms of
168 occlusion, stability of miniplate and fractured fragments, operating time, ease of use, surgical
169 access, and, most importantly, mental nerve paresthesia.

170 An interesting characteristic of this miniplate is its novel design, and fixation of the fracture
171 segments using a minimum of four screws (two on each side of the fracture segment) up to a
172 maximum of nine screws, in a single twin-fork-shaped miniplate. The stability of this
173 configuration is being assessed clinically. These results are not in the scope of this article, and
174 further publications will be submitted when the clinical study is completed.

175 The authors recommend the use of twin-fork miniplates for fixation of transitional zone fractures
176 of the mandible because these plates, according to FE models, produce the lowest stress values
177 and therefore the most stable fixation.

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181 FURTHER STUDIES

182 This was a purely computerized, in-vitro study to evaluate the biomechanical behavior of a
183 newly designed miniplate, using finite element analysis, and compare it with conventional
184 designs. A further in-vivo study regarding its clinical use is underway, and outside the scope of
185 this article. Hence, part two of this study will be purely on a clinical basis, and will soon be
186 submitted after practical and clinical evaluation of this novel twin-fork-shaped miniplate.

187

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191

CONFLICT OF INTEREST

192 The authors have no conflict of interest to declare.

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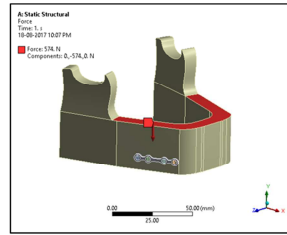
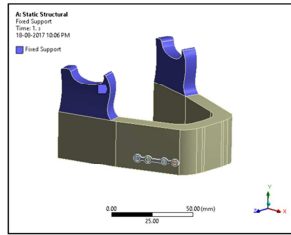
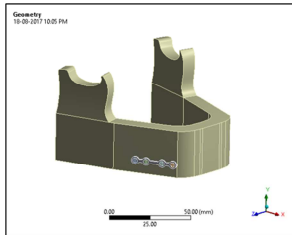
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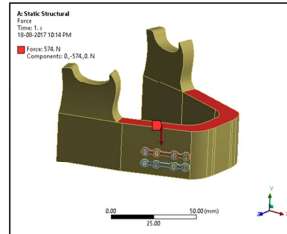
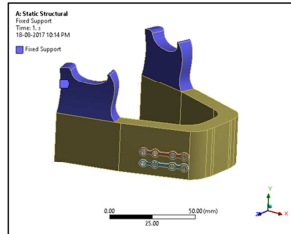
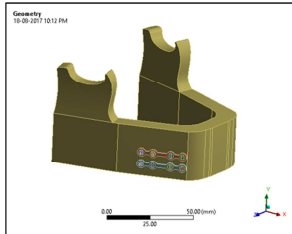
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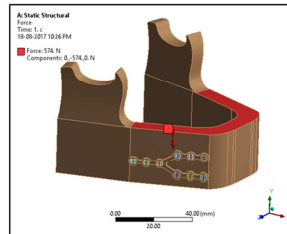
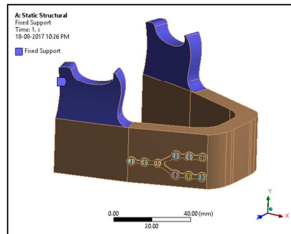
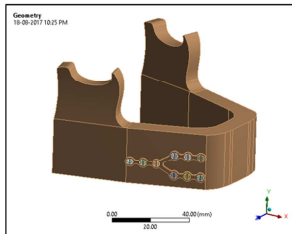
- 228 Figure 1: Finite element models for different configurations of titanium miniplates and screws.
- 229 Figure 2: Meshing of the generated models for various configurations.
- 230 Figure 3: General assembly of the three configurations of titanium miniplate with the host bone.
- 231 The blue markings show the fixed condylar support when the occlusal forces (red area) are
- 232 applied.
- 233 Figure 4: Color grid diagram showing total structural deformation for the three configurations.
- 234 Figure 5: Equivalent von Mises stress distributions along the three miniplate configurations.
- 235 Figure 6 Equalization of stress vectors along the arms of the twin-fork miniplate.



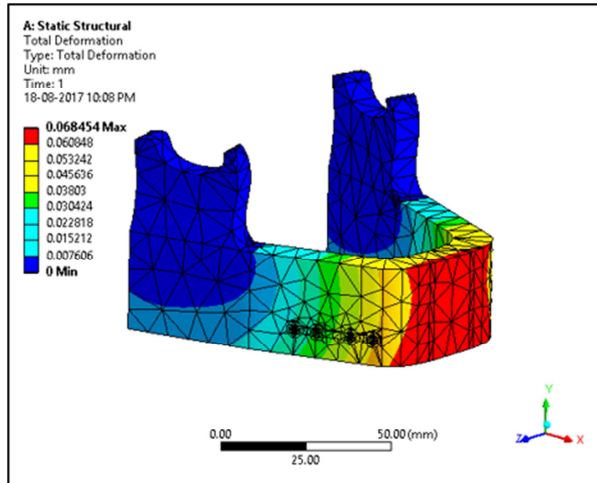
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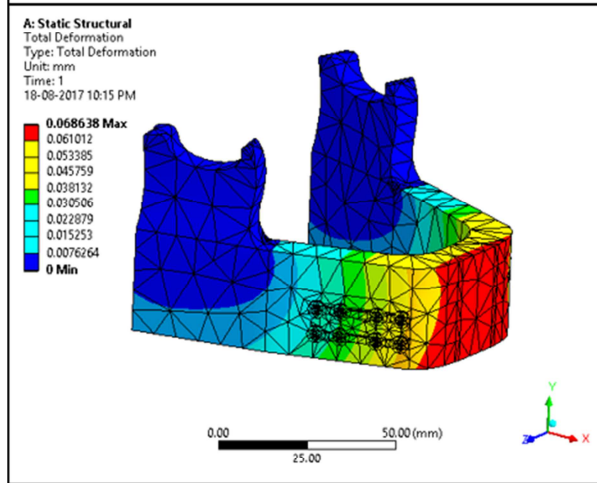
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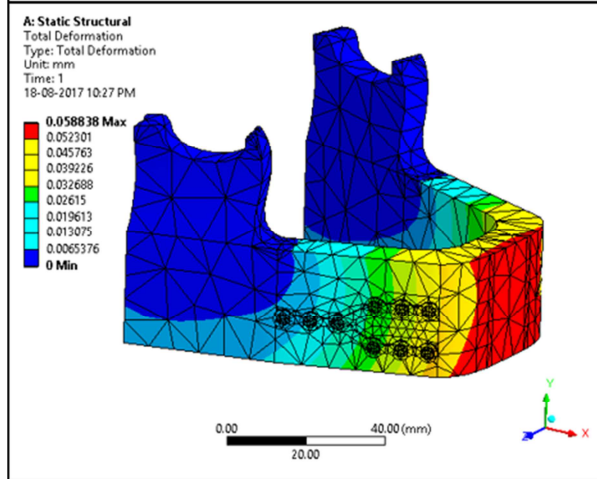
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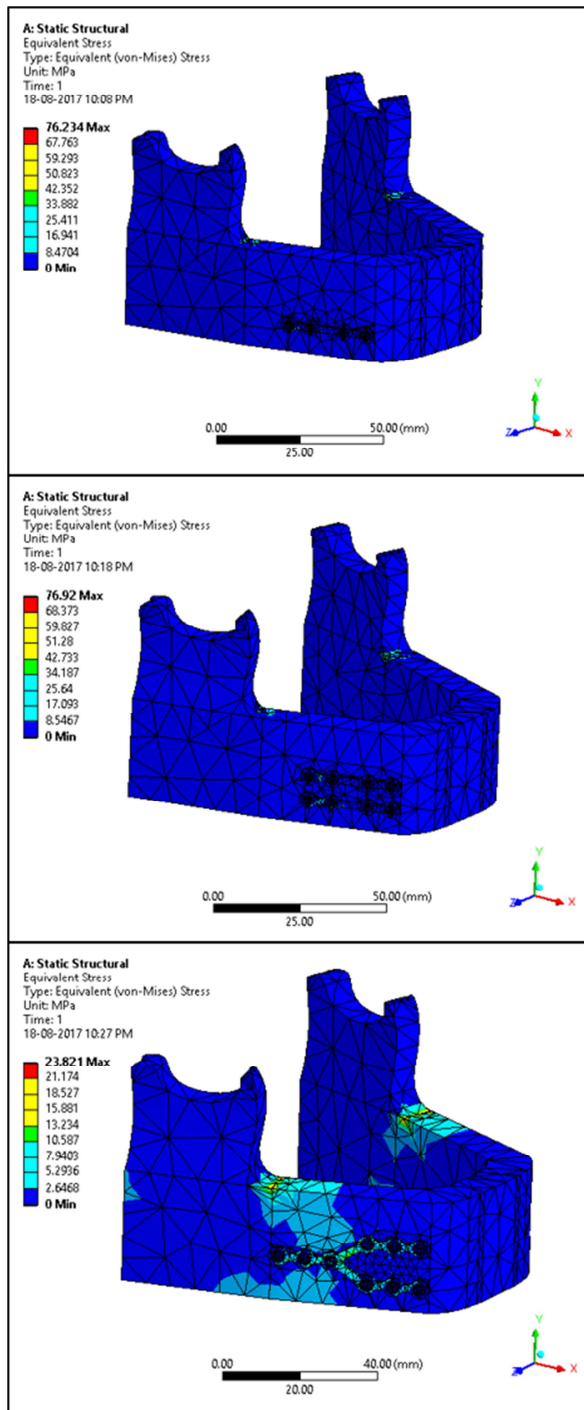
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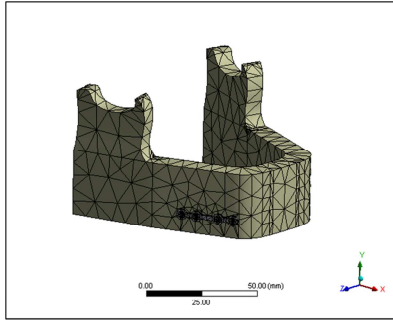
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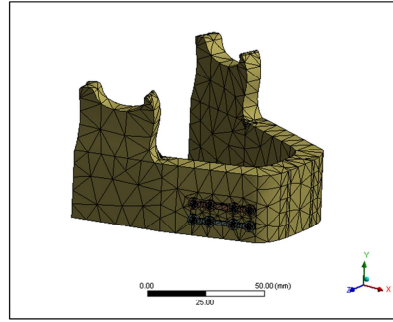
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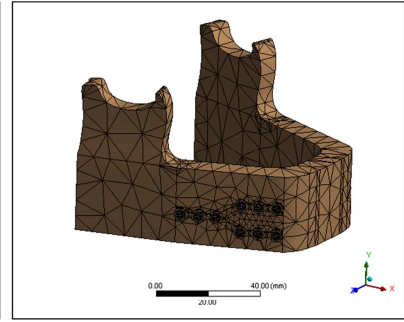
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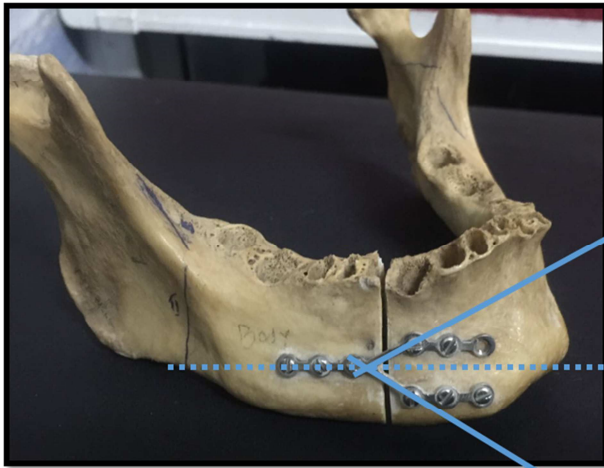


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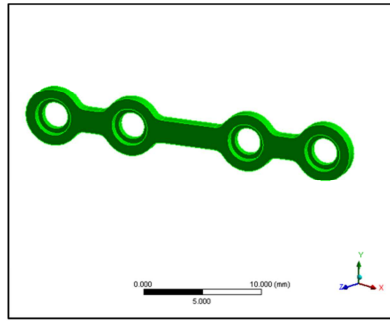
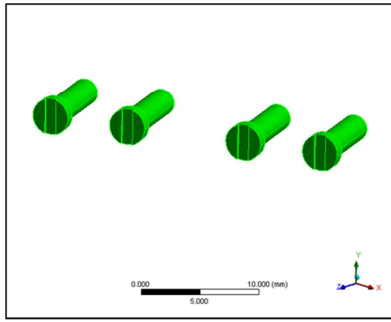
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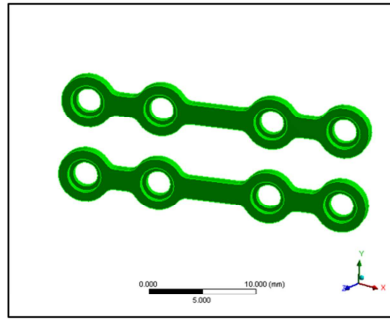
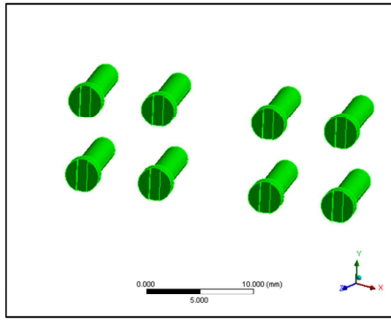


Broad end of the Twin Fork shaped miniplate

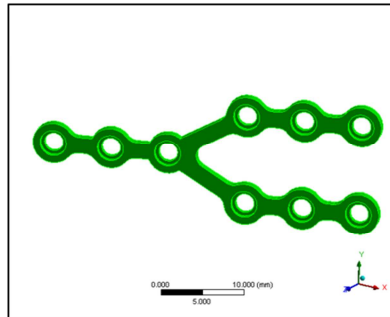
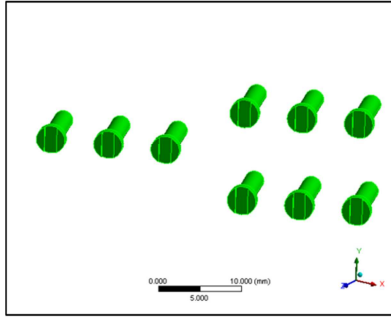
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